Applications of ImmunoPET: Using $^{124}$I-Anti-PSCA A11 Minibody for Imaging Disease Progression and Response to Therapy in Mouse Xenograft Models of Prostate Cancer

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Abstract

Purpose: Prostate stem cell antigen (PSCA) is highly expressed in local prostate cancers and prostate cancer bone metastases and its expression correlates with androgen receptor activation and a poor prognosis. In this study, we investigate the potential clinical applications of immunoPET with the anti-PSCA A11 minibody, an antibody fragment optimized for use as an imaging agent. We compare A11 minibody immunoPET to $^{18}$F-Fluoride PET bone scans for detecting prostate cancer bone tumors and evaluate the ability of the A11 minibody to image tumor response to androgen deprivation.

Experimental Design: Osteoblastic, PSCA-expressing, LAPC-9 intratibial xenografts were imaged with serial $^{124}$I-anti-PSCA A11 minibody immunoPET and $^{18}$F-Fluoride bone scans. Mice bearing LAPC-9 subcutaneous xenografts were treated with either vehicle or MDV-3100 and imaged with A11 minibody immunoPET/CT scans pre- and posttreatment. Ex vivo flow cytometry measured the change in PSCA expression in response to androgen deprivation.

Results: A11 minibody demonstrated improved sensitivity and specificity over $^{18}$F-Fluoride bone scans for detecting LAPC-9 intratibial xenografts at all time points. LAPC-9 subcutaneous xenografts showed downregulation of PSCA when treated with MDV-3100 which A11 minibody immunoPET was able to detect in vivo.

Conclusions: A11 minibody immunoPET has the potential to improve the sensitivity and specificity of clinical prostate cancer metastasis detection over bone scans, which are the current clinical standard-of-care. A11 minibody immunoPET additionally has the potential to image the activity of the androgen signaling axis in vivo which may help evaluate the clinical response to androgen deprivation and the development of castration resistance. Clin Cancer Res; 20(24); 6367–78. ©2014 AACR.

Introduction

There is a significant clinical need for improving the detection of prostate cancer metastases and measuring the response of tumors to systemic therapy. The most common method of screening for prostate cancer, a prostate-specific antigen (PSA) blood test, is notoriously nonspecific and is commonly elevated in benign prostate hyperplasia, prostatitis, and low-risk indolent prostate cancer. Prostate cancer survival is high for the 91% of patients that are diagnosed with local or regional disease and PSA testing is associated with overdiagnosis and treatment of indolent disease (1). On the other hand, prostate cancer is the second most common cause of cancer-related deaths in men and one of the great challenges in treating it is distinguishing the patients who do not need to be treated from those for whom it is life threatening (2). Metastases, and especially bone metastases, represent the primary cause of morbidity and mortality and prostate cancer survival rates fall quickly once the disease has metastasized to distant sites (2). Detection of metastases, therefore, stratifies a subset of patients that need to be treated aggressively and systemically from the large majority of patients where more conservative local therapies or active surveillance is preferred. Following the detection of distant metastases, androgen deprivation becomes the standard-of-care and PSA tests are frequently used to monitor the effectiveness of androgen deprivation and the development of castration-resistant prostate cancer (CRPC).
Clinical detection of prostate cancer metastases and monitoring of the response to androgen deprivation therapy remains inadequate. We have previously developed an engineered anti-PSCA antibody fragment with affinity and pharmacokinetics optimized for imaging, the A11 minibody, and demonstrated high-contrast quantitative immunoPET imaging of PSCA expression. In this work, we investigate the translational applications of A11 minibody immunoPET. We demonstrate detection of bone tumors with higher sensitivity and specificity than 18F-Fluoride bone scans and that the A11 minibody can detect tumor response to androgen deprivation earlier than conventional imaging. These results may directly translate into improved clinical metastasis detection and the ability to noninvasively image the efficacy of androgen deprivation therapy and the development of castration-resistant prostate cancer. We have recently begun a clinical trial to compare A11 minibody immunoPET to bone scans in men with known metastatic disease to investigate this translational potential.

However, PSA levels can only measure the response of the tumors as a whole and cannot determine whether there is an androgen-independent subset of tumors that fails to respond and may necessitate the use of targeted radiation or chemotherapy. There is a need for an imaging modality that can improve the early detection and localization of prostate cancer metastases and image response to androgen deprivation therapy (ADT) to guide therapeutic decision making.

Despite the large influence of bone metastases on patient prognosis and therapy decisions, the current methods of detecting them are unsatisfactory. Most current clinical monitoring for metastases utilizes 99mTc-Methylene diphosphonate (99mTc-MDP) planar or SPECT imaging of bone formation in response to osteoblastic prostate cancer bone metastases, though other methods are at various stages of development (3, 4). Bone scans are clinically recommended for symptomatic patients and asymptomatic men with serum PSA >10–20 ng/mL; however, due to relatively low sensitivity of bone scans and their inability to detect metastases to other sites the presence of prostate cancer recurrence and/or metastasis often must be inferred on the basis of other risk factors such as a rising PSA in a patient who has received a radical prostatectomy (4).

Recently, 18F-Fluoride PET bone scans have shown improved sensitivity over 99mTc-MDP in initial small clinical trials and are currently the subject of a phase III study to determine whether their use improves metastasis detection (5–8). However, while the sensitivity of bone metastasis detection may be improved using 18F-Fluoride bone scans, bone scans are obviously limited to detecting metastases to bone without the ability to image local prostate cancer or metastases to other sites. Bone scans also have considerable false positives due to any benign process that increases bone formation such as trauma and fractures, degenerative diseases (e.g., osteoporosis), Paget disease, and inflammatory processes (e.g., arthritis) which are relatively common in the elderly patients most likely to develop prostate cancer (4, 8). Bone scans, additionally, have difficulty measuring response to therapy due to the flare phenomenon where uptake in bone scan lesions often increases in response to therapy due to bone healing in response to the shrinking tumor. This flare can last for months after successful therapy has been initiated and lesions may continue to appear on bone scans long after the viable tumor has been eliminated (4).

While the mainstay of metastatic prostate cancer therapy is ADT, patients progress to CRPC a median of 2 to 3 years after initiating treatment (9). MDV-3100 (enzalutamide) is a second-generation androgen that has recently won FDA approval for the treatment of CRPC (10). MDV-3100 has continued efficacy in cell lines resistant to other anti-androgens and results in a larger repression of androgen-dependent genes and shorter time period to maximal efficacy than castration in mouse models (11–13). A phase III study of MDV-3100 showed a ≥50% PSA decrease in 54% of patients who had previously failed both ADT and chemotherapy regimens and prolonged median survival 4.8 months over placebo (14). However, many patients do not respond to therapy with MDV-3100 and many initial responders develop resistance rapidly, possibly through the generation of constitutively active splice variants that lack the AR C-terminal ligand binding domain on which MDV-3100 acts (15–17). A method of imaging the activity of the androgen receptor (AR) signaling axis in vivo could lead to improved therapeutic strategies and could allow for targeted radiotherapy or a more prompt transition to alternative androgen deprivation agents or systemic chemotherapy in the patients whose tumors reactivate the androgen-signaling axis.

Prostate stem cell antigen (PSCA) is highly expressed in 83% to 100% of prostate cancers and overexpressed in the great majority of prostate cancer bone metastases (87%–100%) and in many metastases to other sites (67% liver, 67%–95% lymph node; refs. 18–21). Its expression correlates with the Gleason score, tumor invasion, androgen independence, metastasis, and a poor prognosis (21–26). The PSCA promoter contains an androgen response element and PSCA expression is regulated by androgens in the normal mouse prostate (27, 28). Likewise, androgen deprivation decreases PSCA mRNA expression in human high-grade prostatic intraepithelial neoplasia and prostate cancer (29, 30). We have previously shown that immunoPET with an affinity matured 124I-labeled A11 anti-PSCA minibody, an antibody fragment with pharmacokinetics optimized for imaging, can be used for specific and quantitative imaging of PSCA expression in vivo (31–33). We therefore hypothesize that imaging PSCA expression using the A11 minibody may outperform bone scans for imaging prostate cancer bone metastases and allow for imaging changes in PSCA expression in response to androgen deprivation. In this context, A11 minibody imaging of PSCA expression may allow one to detect and localize bone lesions at an earlier stage and allow for monitoring of the response to androgen deprivation therapy.
work, we will compare the sensitivity of the A11 minibody to $^{18}$F-Fluoride bone scans for detecting bone tumors using a naturally PSCA expressing, purely osteoblastic, LAPC-9 intratibial xenograft model. We will also investigate changes in PSCA expression in LAPC-9 subcutaneous xenografts in response to androgen deprivation with MDV-3100 and demonstrate that anti-PSCA A11 minibody immunoPET can image these changes in vivo.

Materials and Methods

Subcutaneous and intratibial xenograft models

LAPC-9 subcutaneous xenografts were passaged surgically in male SCID mice as previously described (34). Single-cell suspensions of LAPC-9 cells were prepared by digesting freshly excised LAPC-9 subcutaneous xenografts in 0.1% Pronase (Sigma) in Iscove modified Dulbecco medium (Gibco) for 18 minutes at room temperature (35, 36). The cells were then passaged through 18 gauge needles and strained through a 70-µm cell strainer (BD Biosciences).

Viable cells ($1 \times 10^5$) were prepared in 10 µL of 1:1 Media: Matrigel and injected into the tibias of anesthetized male SCID mice by drilling a needle through the proximal end of the tibial plateau. Once the needle tip entered the intramedullary space of the tibial metaphysis, the cells were slowly injected and the needle was removed (37). A sham injection, where the needle was inserted using the same method, but only Media:Matrigel was injected, was performed on the contralateral leg. Injections of PSCA-negative 22rv1 cells and 22rv1 × PSCA cells transfeected with PSCA were used, respectively, as negative and positive controls (see Supplementary Materials). All animal experiments were conducted in compliance with a protocol approved by the Institutional Animal Care and Use Committee of the University of California-Los Angeles (Los Angeles, CA).

$^{18}$F-Fluoride and A11 minibody imaging of intratibial xenografts

Intratibial tumor-bearing mice were serially imaged with both bone scans and immunoPET at 4, 6, and/or 8 weeks postintratibial injection. Intratibial xenograft bearing mice were injected with approximately 100 µCi of $^{18}$F-Fluoride in 100 µL of saline via tail vein injection. After an hour of conscious uptake, the mice were anesthetized, their bladders were manually expressed, and the mice were imaged with a 10-minute acquisition on an Inveon microPET scanner (Siemens Preclinical Solutions) followed by a microCT scan (MicroCAT II, Siemens Preclinical Solutions). MicroPET and microCT were automatically coregistered on the basis of empirically determined scanner alignments. All image manipulation and quantification was performed using AmIDE (38). Alignment was manually verified and adjusted using the bladder as a fiduciary marker. Uptake (%ID/g) was then quantified from the coregistered microPET/CT images using microCT isocontour region of interests (≥200 Hounsfield units) to capture a region encompassing either the tumor-bearing tibia or the sham tibia. The mean value of the microPET scan was converted to %ID/g using the decay-corrected injected dose of $^{18}$F-Fluoride and an empirically determined cylinder factor for $^{18}$F.

Either immediately following the $^{18}$F-Fluoride bone scan or the day following the bone scan the intratibial tumor bearing mice were injected with approximately 3 µg $^{124}$I-labeled A11 minibody. Radiolabeling, purification, and immunoreactivity were performed as previously described except for the much higher specific activity used here (~30-50 µCi/µg; ref. 32). Forty-four hours after A11 minibody injection, the mice again received microPET/CT scans. The mice were then either kept for serial imaging at later time points or at the last time point sacrificed for biodistribution as previously described (32). The images were analyzed using the same method as for the $^{18}$F-Fluoride bone scans. No partial volume correction was performed on either the $^{18}$F-Fluoride or $^{124}$I-A11 immunoPET as determining the tumor volume by CT would be too arbitrary to be reproducible and hence only quantification of the entire tibia was performed without attempting to approximate the tumor boundaries. This method provided the additional benefit of allowing direct comparison between the biodistribution and imaging results.

High-resolution ex vivo microCT and histology

After biodistribution, tibias were stored in 10% phosphate-buffered formalin until radioactivity had decayed. The tibias were then analyzed ex vivo by 20-µm resolution microCT (µCT40, SANCO Medical). Volume renderings were generated with OsirX 5.6 (39). The tibia samples were then decalcified and embedded in paraffin and sectioned for histologic analysis. Only those mice with intratibial tumor establishment confirmed by gross and/or histologic analysis were included in the analysis.

A11 minibody imaging of response to therapy with MDV-3100

LAPC-9 subcutaneous xenografts were implanted bilaterally and allowed to grow for 3 weeks. The mice then received a pretreatment A11 minibody immunoPET/CT at 44 hours postinjection as previously described, with the exception that each mouse received a dose of approximately 50 µg of $^{124}$I-A11 minibody (32). Immediately, after the pretreatment scan, the mice were randomized into treatment groups and received either 40 mg/kg MDV-3100 (ChemScene) or vehicle by daily gavage. The vehicle consisted of 300 µL of water with 1% carboxymethylcelulose (Sigma-Aldrich), 0.1% Tween-80 (Sigma-Aldrich), and 1.6% DMSO. After five days of treatment, one mouse from each group underwent a microPET/CT scan to confirm that minimal signal was retained from the first imaging injection, and then all mice were again injected with approximately 50 µg of $^{124}$I-labeled A11 minibody. On the seventh day of treatment, 44 hours post-A11 minibody injection, the mice received a posttreatment scan, following which the mice were sacrificed and biodistribution and microPET image analysis and...
quantification with partial volume correction were performed as previously described (32). The tumors were then fixed and examined histologically (see Supplementary Materials and Methods).

**Quantitative flow cytometry**

LAPC-9 subcutaneous xenograft-bearing mice treated identically to the imaging cohorts, except without the injection of the radioactive tracers, were used for quantitative flow cytometry. After 7 days of treatment with MDV-3100 or vehicle, mice were sacrificed and LAPC-9 tumors were reduced to single-cell suspensions by incubation in 1 mg/mL collagenase IV (Sigma) in HBSS for 1 hour at 37°C. The cells were then passed through 18 and 24 gauge needles followed by a 70 μm cell strainer (BD Biosciences). A total of 5 × 10⁶ LAPC-9 cells from each tumor were incubated in 16 μg/mL [approximately 100 nmol/L] 1G8 mouse anti-PSCA antibody (produced as previously described) followed by 8 μg/mL (approximately 50 nmol/L) Dylight-649 conjugated anti-mouse-Fc (secondary antibody (Jackson ImmunoResearch; ref. 40). After secondary antibody incubation, samples were incubated with Alexa-488 anti-PSMA antibody (FOLH1, BioLegend) and stained with 7-AAD (BD Biosciences). A total of 5 × 10⁹a total of 5 × 10⁶ LAPC-9 cells from each tumor were incubated in 1 μg/mL [1G8 mouse anti-PSCA antibody (produced as previously described)] followed by 8 μg/mL [approximately 50 nmol/L] Dylight-649 conjugated anti-mouse-Fc (secondary antibody (Jackson ImmunoResearch; ref. 40). After secondary antibody incubation, samples were incubated with Alexa-488 anti-PSMA antibody (FOLH1, BioLegend) and stained with 7-AAD (BD Biosciences), as per the manufacturers’ instructions, to allow gating for viable prostate epithelial cells. The final analyzed population was FSC and SSC gated, 7-AADLow, 1G8High, PSMAlow. Acquisition was performed with an LSRII flow cytometer (BD Biosciences) and analysis was performed in FlowJo 9.3.2 (TreeStar). PSCA receptor density was quantified using the QIFIKIT calibration beads (Dako) as per the manufacturer’s instructions.

Statistical analysis

Statistical analysis of both the bone scans and the immunoPET scans in the intratibial model were performed using two-way repeated measure ANOVA with intra-time point significance testing for multiple comparisons performed using the Holm–Sidak method. As the variance of the A11 immunoPET dataset increases significantly as the uptake increases, a log transformation was applied for the homoscedasticity requirement of both ANOVA and Holm–Sidak before significance testing. Significance testing of the MDV-3100 response to therapy model was performed using two-tailed student t tests. The 95% confidence level (P < 0.05) was used for all analysis. Except where indicated otherwise, all values are reported as mean ± SD. All microPET images are displayed as full thickness maximum intensity projections.

**Results**

**Radiolabeling**

¹²⁴I-labeled A11 minibody used in the intratibial xenograft model had a mean specific activity of 23.7 ± 6.5 μCi/μg (n = 8). After purification by size exclusion, the mean purity of the protein injected was 95 ± 5% with immunoreactivity of 62 ± 5%. For the MDV-3100 treatment model, the specific activity for the pretreatment imaging was 1.23 μCi/μg with injected radiochemical purity of 93.8% and immunoreactivity of 72.7%. The posttreatment imaging had specific activity of 2.38 μCi/μg, radiochemical purity of 98.6%, and immunoreactivity of 83.3%.

**Comparison of ¹⁸F-Fluoride ion bone scans and ¹²⁴I-A11 minibody immunoPET in mice bearing intratibial xenografts**

¹⁸F-Fluoride bone scans of mice bearing LAPC-9 intratibial xenografts show a large amount of nonspecific uptake and a qualitative increase in the positive tibia over the negative tibia in only 16.7% of mice at 4 weeks (1/6), 50% (3/6) at 6 weeks, and 50% (1/2) at 8 weeks (Fig. 1A). Quantification of the ¹⁸F-Fluoride bone scans shows an overall increase in tibial uptake of ¹⁸F-Fluoride in the tumor-bearing tibia for all time points in aggregate (P = 0.01, two-way ANOVA), with no trend in increased uptake in the positive tibia over time (P = 0.89). The negative tibias show a large amount of non-specific background uptake, especially in the knee, which leads to a large degree of overlap between the positive and negative tibias and makes quantitative determination of a positive signal due to tumor growth difficult. In fact, the increase in ¹⁸F-Fluoride uptake in the positive tibia only reaches significance in aggregate across time points and fails to reach significance for any individual time point on its own (Fig. 1B).

A11 minibody immunoPET imaging shows intratibial tumor targeting which can be appreciated above blood activity in 67% of mice (4/6) at 4 weeks, 100% of mice (6/6), at 6 weeks and 100% of mice at 8 weeks (2/2) postinjection (Fig. 2A). Imaging of two mice at 8 weeks after intratibial tumor implantation shows that the tumor has invaded through the bone and into the surrounding muscle. Quantification of the serial A11 immunoPET scans shows an overall increase in tibial uptake of the A11 minibody in the tumor-bearing tibia across all time points (P < 0.0001, two-way ANOVA), with an increase in the positive tibia over time (P = 0.001). Because of the high specificity of the A11 minibody and universally low background in normal bone, the positive tibia has significantly higher uptake at all time points (Fig. 2B). The high specificity of A11 minibody, therefore, allows for highly sensitive imaging of bone tumors as any bone uptake above blood can be interpreted as a PSCA-expressing tumor.

Biodistribution of the LAPC-9 mice at 6 (n = 4) or 8 weeks (n = 2) after tumor implantation confirms the results of the immunoPET imaging (Table 1). The 6 week after implantation, mice show an average of 1.51 ± 0.79 %ID/g uptake in the positive tibia and 0.08 ± 0.03 %ID/g in the negative tibia (P = 0.02). At 8 weeks after injection, the uptake is similar with 1.50 ± 0.35 %ID/g in the positive tibia and 0.12 ± 0.00 %ID/g in the negative tibia.

A11 minibody immunoPET of mice bearing negative control 22rv1 intratibial tumors (n = 5) showed no distinguishable intratibial uptake by microPET and showed only a small increase in tibial uptake (0.36 ± 0.19 %ID/g)
compared with the contralateral sham tibia (0.08 ± 0.02 %ID/g) by biodistribution ($P = 0.025$). The small increase in intratibial uptake in the 22rv1 tumor was less than the blood activity (0.40 ± 0.11 %ID/g) and was likely a result of the enhanced permeability and retention effect uptake due to the large degree of nonspecific uptake. Each column displays serial imaging of the same mouse and each is matched with the corresponding A11 immunoPET in Fig. 2.

**Ex vivo microCT and histology**

Gross analysis, *ex vivo* microCT, and histology confirm the presence of an osteoblastic intratibial tumor with spiculated bone formation in each mouse. High-resolution *ex vivo* microCT imaging of the LAPC-9 xenograft-bearing tibias and the sham controls shows spiculated bone formation in the LAPC-9–bearing tibias with sham injected tibias showing normal appearing bone (Fig. 3A). Histology of LAPC-9–bearing tibias shows osteoblastic tumor formation, consistent with previous reports, whereas histology of sham injected tibias shows normal bone marrow (Fig. 3B; refs. 35, 36, 41–46). For mice that grew muscle tumors due
to missed intratibial injections, neither gross analysis nor histology showed the presence of tumor cells in the intramedullary space and on biodistribution only the ipsilateral muscle uptake of A11 minibody was elevated due to the tumor presence and these mice were excluded from the analysis.

**Changes in PSCA expression with MDV-3100 treatment**

Quantitative flow cytometry on digested LAPC-9 tumors following 7 days of treatment with MDV-3100 (40 mg/kg) or vehicle shows that MDV-3100 treatment downregulates PSCA expression 62.8% ± 4.9% (P < 0.0001, n = 4) compared with the vehicle-treated control (Fig. 4A). Quantitative flow finds expression of 4.75 × 10^5 PSCA antigens per cell for vehicle-treated mice, whereas mice treated with MDV-3100 express only 1.65 × 10^5 PSCA antigens per cell.

**ImmunoPET imaging of PSCA downregulation in response to ADT**

Partial volume corrected quantification of the pre-treatment results shows equivalent tumor volumes and
uptake in the two groups before treatment is initiated (2.43 ± 0.42 %ID/g vehicle, 2.65 ± 0.72 %ID/g MDV-3100, \( P = 0.46 \); Fig. 4C). After one week of treatment with MDV-3100, tumor volumes show no significant difference as measured by CT (\( P = 0.54 \)) or by mass (\( P = 0.53 \)). However, following treatment, the A11 minibody uptake in the MDV-3100 treated cohort is 29% lower than in the control group by partial volume corrected microPET (3.70 ± 0.20 %ID/g vehicle vs. 2.61 ± 0.23 %ID/g MDV-3100, \( P < 0.003 \); Fig. 4B and C) and 24.0% lower than in the vehicle-treated controls by biodistribution (Table 2; \( P = 0.03 \)).

Normalizing posttreatment imaging by the pretreatment imaging similarly shows uptake in the MDV-3100–treated group 32% lower than the vehicle-treated group (\( P = 0.0003 \)). However, rather than the MDV-3100–treated

| Table 1. Forty-four-hour biodistribution of \(^{124}\text{I}-\text{A11} \) minibody in mice bearing LAPC-9 intratibial xenografts at 6 and 8 weeks posttumor implantation |
|------------------|------------------|------------------|
| LAPC-9 Intratibial xenograft | 6 weeks | %ID/g ± SD | 8 weeks | %ID/g ± SD |
| Blood | 4 | 0.57 ± 0.15 | 2 | 0.45 ± 0.11 |
| Positive (left) tibia | 4 | 1.51 ± 0.79 | 2 | 1.50 ± 0.35 |
| Sham (right) tibia | 4 | 0.08 ± 0.03 | 2 | 0.12 ± 0.00 |
| Left calf muscle | 4 | 0.45 ± 0.33 | 2 | 2.54 ± 1.26 |
| Right calf muscle | 4 | 0.06 ± 0.02 | 2 | 0.07 ± 0.01 |
| Left femur | 4 | 0.10 ± 0.03 | 2 | 0.14 ± 0.03 |
| Right femur | 4 | 0.10 ± 0.03 | 2 | 0.13 ± 0.00 |
| Liver | 4 | 0.14 ± 0.02 | 2 | 0.28 ± 0.04 |
| Kidney | 4 | 0.24 ± 0.04 | 2 | 0.37 ± 0.04 |
| Spleen | 3 | 0.18 ± 0.08 | | |
| Heart | 3 | 0.21 ± 0.04 | | |
| Lung | 3 | 0.32 ± 0.07 | | |
| Carcass | 4 | 0.12 ± 0.04 | 2 | 0.25 ± 0.05 |
| Pos Tibia: blood | 4 | 2.85 ± 1.49 | 2 | 3.55 ± 1.68 |
| Pos:neg tibia | 4 | 18.98 ± 7.10 | 2 | 12.50 ± 2.98 |
| Pos tibia:muscle | 4 | 27.16 ± 15.5 | 2 | 20.08 ± 8.08 |

At 6 weeks posttumor inoculation, tibias bearing LAPC-9 intratibial xenografts grossly show bone marrow displacement by the tumor and high-resolution ex vivo microCT demonstrates osteoblastic changes in the LAPC-9 injected tibias with normal appearing sham controls (A). Histology of LAPC-9–bearing tibias shows tumor interspersed with osteoblastic bone formation, whereas histology of sham tibias shows normal bone marrow (B).
group decreasing from the baseline scan, we find that the MDV-3100–treated group is not significantly changed from pretreatment (pre:posttreatment ratio 1.10/0.16, \( P = 0.90 \)) and rather the difference posttreatment is due to an increase in the vehicle-treated group between the scans (pre:post treatment ratio 1.61/0.26, \( P = 0.0002 \)).

**Figure 4.** Ex vivo quantitative flow cytometry shows downregulation of PSCA on LAPC-9 tumor cells in response to treatment with MDV-3100 (A). A11 minibody imaging of mice bearing LAPC-9 xenografts treated with MDV-3100 shows decreased tumor uptake in vivo as compared with vehicle controls (B). Quantification of the microPET/CT results shows no difference in tumor volumes or minibody uptake pretreatment (C). However, following a week of treatment, A11 immunoPET shows significantly decreased uptake in MDV-3100–treated mice compared with vehicle controls (\( P = 0.004 \)), whereas CT volume shows no difference between the groups (\( P = 0.54 \)).

**Table 2.** Biodistribution of \(^{124}\)I-A11 minibody in mice bearing LAPC-9 xenografts at 44 hours after injection show decreased uptake in MDV-3100 (40 mg/kg) treated mice compared with vehicle control

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Discussion

An ideal imaging modality for prostate cancer would allow for early detection of metastases that would inform treatment decisions. Imaging of prostate cancer metastases with an imaging agent specific to the tumor itself instead of imaging a downstream process such as bone formation could yield both higher sensitivity and specificity for detecting prostate cancer bone metastases as well as the potential to image local prostate cancer and metastases to other sites. An ideal imaging modality could likewise determine whether a chosen therapy is effective in a patient. While PSA blood tests can measure the response of the tumors in aggregate, they cannot detect whether only a subset of lesions are resistant to therapy. Molecular imaging of AR activity could yield more detailed information regarding individual tumor response to androgen deprivation therapy and development of resistance through the reactivation of AR pathways. ImmunoPET imaging with radiolabeled antibodies targeted to cell surface biomarkers has shown potential for use in this role (13, 31, 47). In previous work, we have shown that 124I-A11 anti-PSCA minibody is capable of specifically imaging PSCA-expressing tumors and that the rapid clearance of the minibody provides excellent imaging contrast at 44 hour postinjection (32, 33). In this work, we demonstrate that A11 minibody immunoPET outperforms the sensitivity and specificity of 18F-Fluoride bone scans for detecting intratibial tumors and can image PSCA downregulation in response to androgen deprivation with MDV-3100 in vivo.

While all LAPC-9 intratibial xenografts in this study show osteoblastic changes and spiculated bone formation on ex vivo microCT and histology, bone scans of LAPC-9 intratibial xenografts show qualitative increases over the sham tibia in only 50% (3/6) mice at 6 weeks after tumor inoculation indicating that the bone scans missed a significant number of osteoblastic lesions. Even at 8 weeks, when the tumors have eroded through the bone and into the surrounding muscle, the 18F-Fluoride bone scans only show a fairly subtle and questionable increase in uptake in 50% of mice (1/2). The low sensitivity of the 18F-Fluoride bone scans may have been due to the intratibial tumors’ proximity to the nonspecific uptake in the tibial growth plate illustrating the problems caused by nonspecific uptake of 111In-DTPA-DTPA. Quantification of the uptake in the tibial growth plate was the least biased method of comparing both A11 immunoPET and bone scans and in vivo and ex vivo measurements using the A11 minibody, the tumor makes up only a fraction of the tibial volume and mass and the %ID/g is decreased by the inclusion of bone and other nontumor tissue in the measurement.

The results of this work indicate that the A11 minibody has the potential to translate into an imaging agent with higher sensitivity and specificity than bone scans for imaging prostate cancer bone metastases in the clinic. In addition, while bone scans are limited to the detection of relatively large bone metastases that cause osteoblastic changes in the surrounding bone, immunoPET imaging can not only image tumors before changes are seen on bone scan, but also image tumors in locations other than bone. Lymph node metastases, lung metastases, liver metastases, and metastases to other locations have been shown to express PSCA and may be imaged with A11 minibody immunoPET adding to its diagnostic value as up to 19% of patients have been found to have only visceral metastases with no bone involvement (18, 19, 48). In addition, PSCA expression has been correlated with tumor stage, metastatic potential, and poor outcomes and imaging of PSCA may help stratify patients with high-risk local disease even in the absence of metastases (21–26).

It has previously been suggested that PSCA may be downregulated in prostate cancer in response to androgen deprivation (27–30). In this work, we found that treatment of mice bearing naturally PSCA-expressing LAPC-9 xenografts with the antiandrogen MDV-3100 causes a significant, nearly 3-fold, downregulation of PSCA in vivo. Imaging of PSCA expression, in addition to helping aid in the localization of metastases, therefore, holds the potential for imaging the activity of the AR signaling axis. After 1 week of treatment, LAPC-9 xenografts treated with MDV-3100 show no significant differences in volume or mass compared with vehicle-treated controls. However, the MDV-3100–treated mice show significantly lower uptake of the 124I-A11 minibody than vehicle controls by both microPET and biodistribution. These results suggest that quantitative imaging of PSCA expression holds the potential to measure the efficacy of ADT in men with prostate cancer before changes in tumor volume can be observed. A11 minibody immunoPET may also be effective in imaging the reactivation of the AR axis upon development of CRPC.

Modeling work by Thurber and Weissleder has suggested that antibody uptake into a tumor will only directly reflect antigen expression when the binding sites are relatively close to saturation and that, otherwise, the antibody uptake will be limited by the rate of antibody extravasation from the vasculature and diffusion into the tissue (49). However, large antibody doses and receptor saturation produces a
blocking effect that reduces imaging contrast and this effect needs to be balanced with the desire for antigen quantitation. While, the dose of A11 minibody in the response to therapy experiments was increased, the PSCA antigens remained relatively far from saturation and hence the decreased uptake of A11 minibody into the tumor (29%) does not directly reflect the degree of PSCA downregulation (63%). The decrease in A11 minibody uptake with MDV-3100 treatment is significant by both microPET/CT and biodistribution. However, the picture is complicated by comparison to the pretreatment imaging. Rather than a simple decrease in A11 minibody uptake in the MDV-3100–treated mice compared with the pretreatment imaging, we instead see an increase in the vehicle-treated mice. A11 minibody uptake increased by 59.7 ± 8.5% (P = 0.0002) in the vehicle–treated mice compared with the pretreatment imaging, whereas the MDV-3100–treated mice show no significant difference between pre- and posttreatment scans (P = 0.90). These results cannot be explained by differences in vehicle and MDV-3100 cohort tumor volumes, masses, or necrosis as no significant differences in these variables were observed (Supplementary Figs. S5–S6). The result was also not due to residual activity from the pretreatment scan as residual activity was minimal and equivalent between the groups. Other explanations for the increase in uptake posttreatment include changes in tumor vascularity and permeability as the tumors of both cohorts grew in the 7 days between scans. We recently published a method that uses diffusion-limited kinetic modeling of dynamic imaging with the A11 minibody tumor to measure permeability, vascularity, and antigen concentration independently which we intend to utilize to address these questions in future works (50). Regardless of the cause of the baseline shift between pre- and posttherapy scans, normalizing of posttreatment uptake values by pretreatment imaging reduces the intracohort variance and results in large effect size compared with the non-normalized data (P = 0.0003). While the explanation for the increase in A11 minibody uptake in the vehicle–treated group between the pre- and posttherapy scans requires further investigation, there was an unequivocal decrease in uptake in the MDV-3100–treated mice compared with the vehicle control that is androgen independence can be quite heterogeneous between different tumors, the determination of whether a subset of tumors fails to respond to treatment could potentially allow for targeted therapies (e.g., external beam radiation) to have a larger role in treating metastatic disease or for a more prompt transition to systemic chemotherapy. We have, therefore, begun investigation of 124I-labeled anti-PSCA A11 minibody in the clinical setting.

Disclosure of Potential Conflicts of Interest
A. Wu is an employer of, has ownership interest in, and is a consultant/advisory board member for ImaginAb, Inc. No potential conflicts of interest were disclosed by the other authors.

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Applications of ImmunoPET: Using $^{124}$I-Anti-PSCA A11 Minibody for Imaging Disease Progression and Response to Therapy in Mouse Xenograft Models of Prostate Cancer

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